

Current Concepts Review

The All-Polyethylene Tibial Component in Primary Total Knee Arthroplasty

- ▶ Outcomes of total knee arthroplasties performed with modern all-polyethylene tibial components have been found to be comparable with or better than those of arthroplasties done with metal-backed modular components in numerous mid-to-long-term follow-up studies, radiostereometric analyses, and the few prospective randomized trials available.
- ▶ Advantages of an all-polyethylene tibial component over a metal-backed modular component include lower cost, avoidance of locking-mechanism issues and backside wear, and increased polyethylene thickness after identical bone resections.
- ▶ Disadvantages of an all-polyethylene tibial component compared with a metal-backed modular component include a lack of modularity, limiting intraoperative options; no option for liner removal in the setting of acute irrigation and débridement; and no option for late liner exchange.
- ▶ Primary total knee arthroplasty with a modern all-polyethylene design can be done in many patients, with substantial cost savings across the health-care system.

Early tibial designs in total knee arthroplasty systems were almost uniformly all-polyethylene, and total condylar arthroplasties (both cruciate-retaining and cruciate-sacrificing or substituting) with use of these tibial components showed survival rates of >90% at the time of long-term follow-up¹⁻⁷. Failure of these early all-polyethylene tibial components was frequently due to aseptic loosening, which was generally attributed to poor surgical technique or flaws in some of the all-polyethylene tibial designs⁸⁻¹⁵. Use of metal-backed tibial components with the total condylar design likewise yielded excellent results^{4,6,16-18}, and with time surgeons perceived advantages with the newly modular components, which provided increased intraoperative flexibility and the ability to apply a porous coating. However, some design modifications with modular metal backing did not fare so well. Less congruent designs that promoted so-called rollback coupled with a heat-pressed, thin polyethylene insert were associated with poor results¹⁹⁻²¹. There were other issues with modular metal backing, including micromotion

secondary to suboptimal locking mechanisms, so-called backside wear, osteolysis, and rising manufacturing costs^{19,22-29}. Thus, potential advantages combined with lower cost prompted renewed interest in modern all-polyethylene tibial designs. Pressure regarding implant cost in a rapidly changing health-care environment may more directly impact surgeons in the future. The purpose of this review is to outline the clinical rationale behind the use of all-polyethylene tibial designs, the design criteria necessary for success, and the implications of more widespread use of the all-polyethylene tibial design.

Historical Background

Designs favoring articular congruency have generally been the deciding factor in the success or failure of all-polyethylene tibial

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components. In particular, suboptimal results with the University of California, Irvine (UCI) all-polyethylene tibial design may have been important in the development of metal-backed tibial components. These relatively thin, flat, u-shaped all-polyethylene tibial components failed at rates of 7% to 17.4% in clinical series with two to eight years of follow-up^{9,10,15}. The frequent finding of polyethylene deformation (cold flow) of tibial components retrieved at revision, the fact that only 5.0 and 7.5-mm thicknesses were available, the relative lack of articular congruency, and the limited tibial surface coverage were major concerns raised in these studies. Improper technique, including poor component alignment, poor component fixation, and soft-tissue imbalance, were also identified as causes of early failure¹⁵ (Fig. 1).

In the time frame in which these design and technique failures occurred, biomechanical and finite-element-analysis studies suggested a role for metal backing of the tibial component. Proposed advantages of a metal-backed tibial component included decreased bending strains in the stem, reduced compressive stresses in the cement and cancellous bone beneath the baseplate (especially during asymmetric loading), and effective distribution of eccentric load onto a large area of the proximal

part of the tibia³⁰⁻³⁷. Metal backing was also thought to act in a heat-sink capacity, lowering the overall temperature during curing at the bone-cement interface³⁸. Although initially metalbacked monoblock designs were predominant, as metalbacked tibial designs incorporated modularity, surgeons saw advantages to the increased intraoperative flexibility, the ability to use longer stems and modular augments, and the ability to apply porous coating if desired. Gradually, all-polyethylene tibial components were largely abandoned in favor of metalbacked tibial components, which have become predominant in total knee arthroplasty^{28,29,39-41}. According to the Hospital Purchasing Database⁴¹, which contains data from 100 to 200 large U.S. hospitals, usage of all-polyethylene tibial components ranged from 0.8% to 1.5% of all total knee arthroplasties annually between 2003 and 2008. Similarly, an all-polyethylene tibial component was used in only 0.6% (248) of the 42,791 cases recorded in the National Joint Registry³⁹ from England and Wales in 2004. In the HealthEast Joint Registry, which contains data from institutions with surgeon advocates of allpolyethylene tibial components^{28,40}, usage is recorded as ranging between 3.9% and 12.9% annually and was 10.7% in 2008.

Reconsideration of the All-Polyethylene Tibial Component

Like the all-polyethylene tibial component, metal-backed tibial components have been associated with excellent results when used with the total condylar design^{4,6,16-18}. Thus, the question arises: What has led to the recent reconsideration of the allpolyethylene tibial design? Distinct from monoblock metal backing, other design modifications that incorporated the concept of a metal-backed tibial component occasionally proved problematic with longer follow-up. As Engh et al.¹⁹



Fig. 1

A standing anteroposterior radiograph of two different all-polyethylene tibial designs used in the past shows failure related to tibial subsidence, improper soft-tissue balance, or some combination of these mechanisms.

commented: “The potentially negative aspects of these design changes (a less congruous interface, metal-backing, screw holes in the baseplate, and modular inserts) were not at first fully appreciated.” The assumption of improved survivorship and clinical performance with metal-backed tibial components (as compared with all-polyethylene tibial components), as predicted

by some of the biomechanical analyses³⁰⁻³⁸, has been difficult to demonstrate in clinical practice. Moreover, even the perceived advantage of modularity has been questioned in more recent studies²²⁻²⁵. These concepts (modularity and biomechanical features) as well as issues surrounding cementless fixation and implant cost deserve greater scrutiny.

Modularity of Components

The advantages and disadvantages of modularity with a metalbacked tibial component seem clear to most surgeons (Table I).

The potential for exchange of the polyethylene insert is a presumed advantage, especially in younger patients, who might require revision in the future. However, at least three separate studies have identified the relatively limited role of isolated polyethylene exchange for addressing wear⁴²⁻⁴⁴. In a multicenter study, Bert et al.⁴⁵ reviewed sixty-two revision total knee arthroplasties performed secondary to failure of the modular tibial insert. In fifty-five cases (89%), there was obvious scoring or other damage to the femoral and/or tibial components, necessitating revision of one or both components. A simple liner exchange seems appealing but implies that the mode of wear failure has not involved axial malalignment necessitating complete revision and has been detected before osteolysis or severe wear has compromised the metal backing. Two recent studies with short to midterm follow-up do support the practice of isolated liner exchange, with or without bonegrafting, in selected cases with well-fixed and aligned femoral and tibial components^{46,47}. Full revision of well-fixed total knee components can lead to substantial bone loss, and modular polyethylene exchange may therefore be a reasonable option in certain cases.

The metal-backed tibial component also allows a final stability trial after the components have been cemented in place. In the senior author's experience (T.J.G.) in a teaching institution, the lack of this option has not been a limiting feature of the all-polyethylene tibial component, as revisions due to instability were rare with both designs in randomized trials^{28,48,49}. The metal-backed tibial design offers different stem and augment options that cannot be added to the allpolyethylene tibial component, but these options are seldom needed in a primary total knee arthroplasty and their necessity is routinely determined with preoperative templating. Moreover,

nothing in the current all-polyethylene tibial designs precludes the surgeon from switching to a metal-backed tibial component intraoperatively if conditions dictate. In addition, when a patient requires removal of the tibial component alone, an all-polyethylene tibial component can be removed more easily, and with less chance of damaging a retained femoral component, by simply cutting the polyethylene stem.

Micromotion at the liner-tray interface of modular components is known to liberate polyethylene debris, despite the apparent security of the liner-capture mechanism^{25,50-53}. The size of the liberated debris is within the biologically active range with respect to macrophage stimulation⁵⁴, which might account for the increased synovitis and osteolysis seen after the introduction of modularity²⁶ (Figs. 2-A, 2-B, and 2-C). In a study of modular tibial baseplates, Parks et al.²⁵ found that even at the lowest loading level of 100 N all inserts moved an average of at least 100 mm relative to the baseplate and at 400 N all inserts moved an average of at least 500 mm in at least one direction. In a separate retrieval study of 124 polyethylene

TABLE I Advantages and Disadvantages of All-Polyethylene and Modular Metal-Backed Tibial Components

	All-Polyethylene	Metal-Backed
Advantages	<ul style="list-style-type: none"> Lower cost Excellent clinical results and long-term survivorship Avoidance of locking-mechanism issues and backside wear Osteolysis rarely reported Increased polyethylene thickness with same amount of bone resection as used for same-size metal-backed component Relative ease of isolated tibial component revision 	<ul style="list-style-type: none"> Modularity with intraoperative flexibility Excellent clinical results and long-term survivorship Ability to use porous coating if desired Possibility of late liner exchange Potential for use of minimally invasive techniques Smaller shelf inventory
Disadvantages	<ul style="list-style-type: none"> Lack of modularity limits intraoperative options Few options for cementless use No options for liner removal in procedures involving acute irrigation/débridement No options for late liner exchange Potential difficulty with removing posterior extruded cement Increased shelf inventory 	<ul style="list-style-type: none"> Higher cost Locking-mechanism issues, backside wear Higher prevalence of osteolysis Decreased polyethylene thickness with same amount of bone resection as used for same-size all-polyethylene component Relative difficulty with isolated tibial component revision



Fig. 2-C

Cystic lesions representing osteolysis are seen surrounding the tibial component (Fig. 2-A) and femoral component (Fig. 2-B) of a modular total knee replacement in conjunction with articular surface wear of the polyethylene insert (Fig. 2-C).

tibial inserts, moderate-to-severe backside wear was frequently observed in all of the twelve different designs studied, independent of the capture mechanism²³. The average volumetric wear rate was $138 \pm 95 \text{ mm}^3/\text{yr}$ ²². Similarly, in a report on four different tibial baseplate locking mechanisms, Li et al.⁵³ found clear backside wear in twenty-four (44%) of fifty-five inserts, and the manufacturer's stamped markings had been removed completely from eight of the twenty-four (Fig. 3). How mobile-bearing designs and improvement in fixed-bearing locking mechanisms, sterilization methods, and the polyethylene itself might affect this area of active research remains to be demonstrated.

The results of studies of monoblock metal-backed tibial components might reasonably be expected to elucidate the issue of modularity in total knee arthroplasty. Although there is a lack of Level-I and Level-II studies comparing metal-backed monoblock and modular designs, numerous retrospective cohort studies⁵⁵⁻⁵⁸ have shown monoblock metal-backed tibial designs to have either better or equal survivorship, and be associated with less osteolysis, than modular metal-backed tibial designs. However, the cost differential between monoblock metal-backed and all-polyethylene tibial components still favors the all-polyethylene design, and monoblock metal-backed tibial components are not featured in most manufacturers' product lines.

Modularity does have benefits in some revisions performed to address instability, in which an insert with additional constraint may be employed⁵⁹⁻⁶¹. It may also have a role in revisions due to early acute hematogenous infection⁶², as some surgeons suggest that liner exchange allows more complete synovectomy and access to the implant interface—an interface that does not exist with monoblock all-polyethylene tibial components. However, recent research has demonstrated a limited role for open débridement and polyethylene exchange in the setting of presumed acute infection, in which multiple other variables contribute to success or failure⁶³⁻⁶⁵. In a meta-analysis by Silva et al.⁶⁵, débridement and insert exchange successfully controlled the infection in less than one-third (173; 32.6%) of 530 cases.

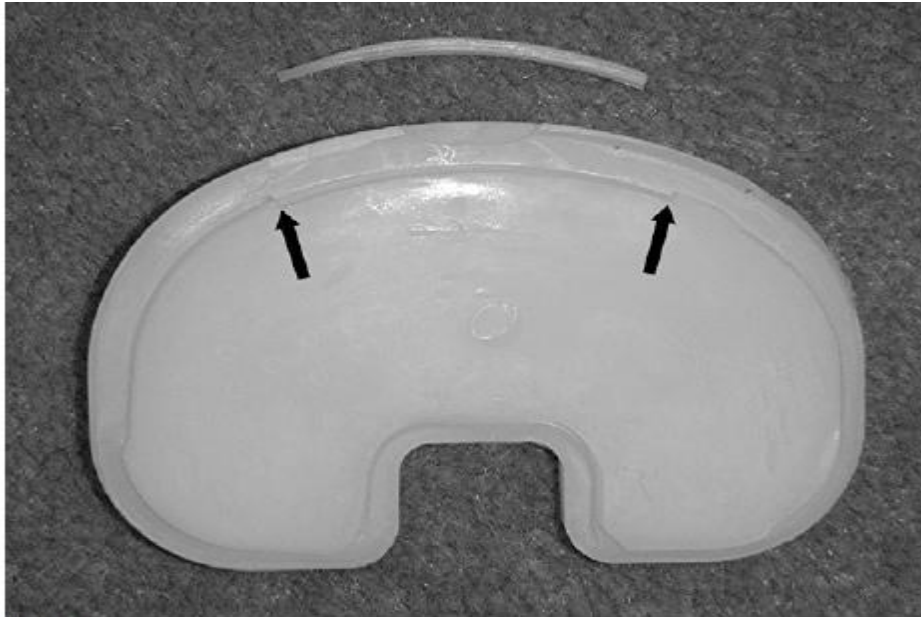


Fig. 3

A retrieved modular insert shows burnishing associated with backside wear and a broken peripheral capture mechanism. The arrows denote where the polyethylene of the capture mechanism has separated from the insert.

Biomechanics of Metal Backing

The longevity of the polyethylene articulating with the femoral component has been shown to be affected by numerous factors, including the duration of implantation and the thickness, conformity, and specific formulation of the polyethylene used^{66,67}. Metal backing reduces the thickness of the polyethylene insert that is used compared with an identically sized allpolyethylene tibial component, forcing the surgeon to choose between additional bone resection and decreased polyethylene thickness when selecting the metal-backed tibial component. As long as the actual insert thickness is at least 8 mm, metal backing should have little influence on surface wear^{66,68}. Theoretically, an all-polyethylene tibial component of 8 to 10 mm in thickness would be more durable than a metal-backed tibial component of identical thickness, accounting for the thickness of the baseplate. In their ten-year follow-up study of a widely used metal-backed total knee arthroplasty design, Schai et al.⁶⁹ noted that the 8-mm insert that was commonly used had an actual polyethylene thickness of 5.5 mm and that no liner of >10 mm in thickness was revised for wear. Although, on the basis of the aforementioned biomechanical

studies^{31,66,70}, metal-backed tibial components are perceived to have the advantage of improved load distribution to the proximal part of the tibia, the interface between the tibial component and the osseous tibia may be adversely affected by the metal backing. The increased stiffness of the metal baseplate increases the tensile forces on the plateau opposite the side subjected to compressive loading (the so-called teetertotter or see-saw effect)³¹. Therefore, as long as a central stem is used, an all-polyethylene tibial component may be less prone to this effect than a similarly designed metal-backed tibial component, or at least this may be the case for components of up to 13 mm in thickness. Thicker all-polyethylene tibial components can be as stiff as similarly sized metal-backed tibial components⁸.

One method for evaluating the findings of various in vitro biomechanical or finite-element-analysis studies over relatively brief time frames in vivo is radiostereometric analysis^{71,72}. Radiostereometric analysis has extremely high resolution and has been shown to predict the risk of future aseptic loosening on the basis of initial implant migration. Randomized clinical studies employing radiostereometric analysis have not shown metal-backed tibial components to have improved fixation or decreased subsidence compared with all-polyethylene tibial components, irrespective of bone quality^{12,29,73-78}. In a prospective randomized trial involving radiostereometric analysis of the coronally flat Freeman-Samuelson total knee arthroplasty design (Sulzer Orthopaedics, Zug, Switzerland), Adalberth et al.⁷⁴ found no difference ($p > 0.05$) in migration between twenty all-polyethylene tibial components and eighteen metal-backed tibial counterparts. The all-polyethylene tibial implants showed no migration between one and two years after the operation, a finding known to be of positive prognostic importance with regard to predicting future aseptic loosening⁷². In a similar study of the AGC (anatomic graduated component) total knee arthroplasty design (Biomet, Warsaw, Indiana), the same group of authors⁷⁵ reported the migration of all-polyethylene tibial components to be on a par with, or sometimes less than, that of metalbacked tibial components ($n = 17$). Rotational motions of the all-polyethylene tibial components were as low as, and maximum lift-off was significantly lower than ($p = 0.017$), those of the metal-backed tibial components.

Cementless Fixation

Cementless total knee arthroplasty technology was an outgrowth of the emerging use of cementless fixation in total hip arthroplasty and the ability to apply porous substrates to newly modular metal-backed designs. Metal-backed modular tibial components allow cementless fixation with a porous coating whereas all-polyethylene tibial designs typically do not. Advocates of cementless fixation of total knee arthroplasty components would therefore have little interest in all-polyethylene tibial designs. However, most studies directly comparing cemented and cementless designs have generally favored the former since cemented implants had equal survivorship and cost less⁷⁹⁻⁸¹. Similarly, the results of studies based on the Swedish Knee Arthroplasty Register, the Mayo Clinic registry, and the HealthEast Joint Registry have also favored cemented over cementless fixation in total knee arthroplasty⁸²⁻⁸⁵. Unless a surgeon is committed to a cementless total knee arthroplasty design for reasons other than survival of the implant (e.g., avoidance of the use of cement in minimally invasive approaches), a cemented all-polyethylene tibial component can be used in an uncomplicated primary total knee arthroplasty with favorable long-term survival.

Implant Cost

Surgeons are increasingly called on to help manage the rising costs of health care^{86,87}, and the American Academy of Orthopaedic Surgeons has issued a position statement that endorses that role^{88,89}. The cost saving that could be realized with the use of an all-polyethylene tibial component in selected patients is substantial (20% to 50% compared with the cost of its metal-backed tibial counterpart)^{28,29,40,48,49,90-92}. In a randomized study by one of us (T.J.G.) and colleagues^{48,49}, the all-polyethylene tibial component cost, on the average, US\$675 less than a metal-backed tibial component of the same design. In a community registry study²⁸, one of us (T.J.G.) and colleagues reported an average negotiated cost of \$3035 for metal-backed tibial implants and \$2078 for all-polyethylene tibial implants. Savings of approximately \$95,000 for every 100 patients receiving an all-polyethylene tibial component were realized. If all patients seventy-five years of age or older had received an all-polyethylene tibial component, the inflation-adjusted savings on implant costs alone would have been \$1.17 million over fourteen years. If all patients older than seventy years of age

(43% of the patients treated with a total knee arthroplasty in this registry database in 2005) had received an all-polyethylene tibial component, the savings would have been \$2.15 million. Pomeroy et al.⁹² showed a 20% to 30% (more than \$75,000) decrease in implant costs when all-polyethylene tibial components rather than metal-backed tibial components of the same design were selectively used for patients over seventy years of age. Healy et al.⁹⁰ noted that, with the implementation of a clinical pathway and knee-implant standardization program, the use of all-polyethylene tibial implants increased from 0% in 1992 to 14% in 1995, which was one of the factors that reduced the average implant cost by 24.7% in 1995. Similarly, Muller et al.²⁹ estimated that, of 42,791 primary total knee arthroplasty procedures recorded in the Annual National Joint Registry Report³⁹ in England and Wales in 2004 (60% of the total performed in that year), only 248 were done with an all-polyethylene tibial component. If 50% of the approximately 70,000 primary total knee arthroplasties undertaken each year had been done with an all-polyethylene tibial implant, a net savings of £21 million (approximately 39 million in 2004 U.S. dollars) per annum would have resulted. (The cost was £1139 for the metal-backed tibial component and £541 for the all-polyethylene tibial component.)

Although some have noted that stocking both all-polyethylene and metal-backed tibial components increases inventory costs⁹³, this cost appears to be minor in comparison with the potential savings. The results of cost-effectiveness analysis would of course depend on the relative rates of revision of modern metal-backed tibial and all-polyethylene tibial designs as noted in direct comparative studies. Since such studies are infrequent and extant studies have generally shown the survival of all-polyethylene tibial components to be equal or superior to that of metal-backed tibial components, and the cost to be less, further analysis may not be warranted.

Between 2000 and 2004, of the top ten surgical procedures in the United States, total knee arthroplasty had the most rapid increase in inpatient hospital cost for all payers⁹⁴. With the volume of total knee arthroplasty increasing and healthcare reform a looming issue in the United States, there have been numerous proposals for bundling the episode of care of total knee surgery^{94,95} that may make the all-polyethylene tibial component an even more cost-effective option.

Clinical Studies Comparing All-Polyethylene and Metal-Backed Tibial Designs

There is a paucity of evidence-based research directly comparing the clinical performances of all-polyethylene and metal-backed tibial components. In a prospective, randomized, controlled trial consisting of 316 total knee arthroplasties in 290 patients, one of us (T.J.G.) and Bowman⁴⁸ found no difference in clinical or radiographic outcomes between the two groups at a mean of forty-nine months postoperatively. At eight to twelve years (mean, 115 months) postoperatively, with one patient lost to follow-up, 167 total knee replacements (ninety-seven with an all-polyethylene tibial component and seventy with a metal-backed tibial component) remained⁴⁹. There were no differences in knee function⁹⁶, range of motion, stability, or radiographic parameters between the groups. The ten-year rates of survival of the all-polyethylene tibial components were 91.6% with revision for any reason as the end point and 100% with aseptic loosening as the end point. The rates of survival of the metal-backed tibial components were 88.9% and 94.3%, respectively ($p = 0.04$). Similarly, in a randomized trial of forty-one patients, Muller et al.²⁹ found no difference in the findings on radiostereometric analysis, Oxford knee scores⁹⁷, Short Form-12 scores⁹⁸, alignment, or range of motion at twenty-four months postoperatively, although the study was underpowered to identify a difference in these parameters. In a prospective, randomized, controlled study of 312 total knee arthroplasties in 273 patients, 136 fixed-bearing allpolyethylene tibial components were compared with 176 mobilebearing rotating-platform metal-backed tibial components of the same design⁹⁹. After a minimum of two years (mean, fortytwo months) of follow-up, no significant difference ($p \nless 0.05$) was noted between the groups with regard to the Knee Society pain or clinical scores⁹⁶, WOMAC (Western Ontario and McMaster Universities Osteoarthritis Index) scores¹⁰⁰, selected Short Form-36 scores¹⁰¹, range of motion, or revision rates. In a prospective study of data on 443 total knee arthroplasties in 378 patients recorded in a community-based registry, one of us (T.J.G.) and colleagues²⁸ found the rate of survival of all-polyethylene tibial components at 14.3 years to be 99.4% with revision for any reason as the end point and 99.7% with revision due to aseptic loosening or wear as the end point. The cumulative revision rate of 1% for the allpolyethylene

tibial components was better ($p = 0.02$) than the 4.9% rate in a comparative cohort of 4977 metal-backed tibial

components in 4109 patients during the same time frame.

However, once the hazard ratio was adjusted for the variables that met the confounder criteria (age and cruciate-retaining versus cruciate-substituting design), there was no difference in the risk of revision between the all-polyethylene and metalbacked tibial implants.

In a retrospective review of eighty-one all-polyethylene tibial components (total condylar or cruciate condylar design) in fifty-nine patients (mean age, seventy-nine years) followed for a mean of 8.1 years, Pagnano et al.⁹³ noted the survival rate at fourteen years to be 100% with symptomatic loosening as the end point and 98% with a revision for any reason as the end point. A number of corroborative studies have been published in recent years. Most have been retrospective and chronologically biased toward the metal-backed tibial components, which typically were implanted later in the surgeon's experience with the same total knee arthroplasty, or the authors used either matched-pair analysis or nonrandomized cohorts in their comparison of various all-polyethylene and metal-backed tibial designs. None of these studies showed superiority of the metal-backed tibial design, and the authors have universally encouraged greater use of all-polyethylene tibial components (see Appendix)^{8,14,26,91,92,102-105}.

Most of the above studies comprise relatively elderly populations (sixty years of age or older), and all-polyethylene tibial components have not been evaluated extensively in younger patients. However, in a review of the results of fiftyfour total knee arthroplasties performed in thirty-eight patients who were less than sixty years of age, Ranawat et al.¹⁰⁶ reported excellent clinical performance and survivorship at a mean of five years postoperatively. There was no radiographic evidence of component loosening, progressive radiolucent lines, or osteolysis.

Role of All-Polyethylene Tibial Design and Surgical Technique

It would appear that the ideal design for all-polyethylene tibial components would have round-on-round conforming or moderately conforming articulation surfaces. In a finite element-analysis study, Bartel et al.³¹ found that compressive stresses on the cancellous bone were increased substantially when the load was applied to a single plateau; however, when loading was distributed more equally on both plateaus, the stresses in the cancellous bone under the all-polyethylene tibial component was nearly equal to those in the cancellous bone under the metal-backed tibial component. The stresses were greatest when there was extreme edge-loading, which was typically seen when there was varus-valgus tilt of implants with a flat-on-flat geometry in the coronal plane. In a study of 536 flat-on-flat nonconforming coronal design all-polyethylene tibial components in 405 patients, Faris et al.¹¹ reported a failure rate of 68% at ten years. Fifty-eight (73%) of seventy-nine failures occurred in association with loosening or collapse of the bone beneath the medial tibial plateau. Ritter¹³ had earlier reported a one-year revision rate of 3% and a 15% rate of radiographic evidence of collapse of the medial tibial plateau in the same study population. In addition to the flat coronal geometry, the I-beam stem and undersurface of this particular design do not offer the same mechanical means of fixing the device in the cement as do the undercuts in other designs. This design flaw has been acknowledged^{11,13}, and all-polyethylene tibial designs that provide better coronal conformity^{28,48,49} theoretically should not have the same failure mode. In contrast, metal-backed components of the same design have had excellent long-term survival, consistent with the findings of finite element analysis⁵⁵. A recent in vitro wear-simulator study¹⁰⁷ also suggested that the newer gamma-irradiated-in-a-vacuum, moderately cross-linked polyethylene inserts combined with a smooth cobalt-chromium baseplate may show low wear rates even with a low-conformity, flat design. However, the authors of the study did not test an all-polyethylene tibial design, and moderate congruity still appears prudent in all-polyethylene tibial designs.

Although round-on-round designs help to minimize lift-off and edge-loading, the surgical technique is primarily responsible for reduction of lift-off since this can occur with any design and is a function of overall limb alignment^{108,109}. The

surgical instrumentation system that the surgeon favors for implantation of a metal-backed tibial design is typically employed to implant an all-polyethylene tibial design from the same manufacturer. Tibial drills or punches may vary slightly between the designs. The trials of the components are identical, but since the all-polyethylene tibial component is nonmodular the surgeon must be satisfied with the findings of the intraoperative examination of stability prior to cementation. We recommend that surgeons using a posterior-stabilized all-polyethylene tibial system cement the femoral component initially during the one-stage cementing process, since the post of an all-polyethylene tibial component of a posteriorstabilized design may interfere with easy seating of the femoral component. In our experience, exposure has not been a problem despite skin incisions averaging 12 cm and use of a variety of so-called less invasive approaches to the extensor mechanism. Any posterior cement is cleared prior to reduction of the femur on the all-polyethylene tibial implant. We have limited experience with cruciate-retaining all-polyethylene tibial designs but in those settings the tibial component should be cemented first during the one-stage cementing process. Computer navigation techniques may ultimately prove to be of assistance in eliminating failures of all-polyethylene tibial components secondary to poor alignment or instability related to surgical technique.

Overview

In conclusion, all-polyethylene and metal-backed tibial components have both advantages and disadvantages. The advantages of the metal-backed tibial component proposed on the basis of in vitro biomechanical studies have not necessarily translated into improved results in either early radiostereometric analyses or long-term clinical studies. Numerous studies support the concept that a stemmed cemented all-polyethylene tibial design with a minimal thickness of 8 mm favoring articular congruency and available in multiple sizes remains practical for primary knee arthroplasty in the majority of patients. The metal-backed tibial component offers greater intraoperative flexibility in that a final trial may be performed after the components are cemented in place. The metalbacked tibial component also offers options of stems and augments, which cannot be added to the all-polyethylene tibial component, but these options are not used for the

majority of total knee arthroplasties and the need for them is typically identified during preoperative planning. Nothing in the most current total knee arthroplasty designs precludes the surgeon from changing the intraoperative plan and using a metal-backed tibial component if conditions dictate. The appeal of liner exchange in certain situations is obvious; however, if the entire tibial component must be removed, an all-polyethylene implant can be removed more easily and with less chance of damaging a retained femoral component. The contribution of backside wear to overall volumetric wear and subsequent osteolysis is essentially nonexistent with use of all-polyethylene tibial designs. Finally, the issue of cost clearly favors the all-polyethylene tibial component, and evolving health-care reform models may increasingly force the surgeon to participate in the cost debate. In light of the current basic-science, clinical, and economic evidence, equal consideration should be given to the use of all-polyethylene and metalbacked tibial implants in primary total knee arthroplasty.

Appendix

A table presenting clinical studies comparing allpolyethylene and metal-backed tibial total knee arthroplasty components is available with the electronic version of this article on our web site at jbjs.org (go to the article citation and click on “Supporting Data”).

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References

1. Gill GS, Joshi AB, Mills DM. Total condylar knee arthroplasty. 16- to 21-year results. *Clin Orthop Relat Res.* 1999;367:210-5.
2. Ranawat CS, Flynn WF Jr, Saddler S, Hansraj KK, Maynard MJ. Long-term results of the total condylar knee arthroplasty. A 15-year survivorship study. *Clin Orthop Relat Res.* 1993;286:94-102.
3. Rodriguez JA, Bhende H, Ranawat CS. Total condylar knee replacement: a 20-year followup study. *Clin Orthop Relat Res.* 2001;388:10-7.
4. Scuderi GR, Insall JN, Windsor RE, Moran MC. Survivorship of cemented knee replacements. *J Bone Joint Surg Br.* 1989;71:798-803.
5. Vince KG, Insall JN. Long-term results of cemented total knee arthroplasty. *Orthop Clin North Am.* 1988;19:575-80.
6. Font-Rodriguez DE, Scuderi GR, Insall JN. Survivorship of cemented total knee arthroplasty. *Clin Orthop Relat Res.* 1997;345:79-86.
7. Ranawat CS, Boachie-Adjei O. Survivorship analysis and results of total condylar knee arthroplasty. Eight- to 11-year follow-up period. *Clin Orthop Relat Res.* 1988;226:6-13.
8. Apel DM, Tozzi JM, Dorr LD. Clinical comparison of all-polyethylene and metalbacked tibial components in total knee arthroplasty. *Clin Orthop Relat Res.* 1991;273:243-52.
9. Ducheyne P, Kagan A 2nd, Lacey JA. Failure of total knee arthroplasty due to loosening and deformation of the tibial component. *J Bone Joint Surg Am.* 1978;60:384-91.
10. Evanski PM, Waugh TR, Orofino CF, Anzel SH. UCI knee replacement. *Clin Orthop Relat Res.* 1976;120:33-8.
11. Faris PM, Ritter MA, Keating EM, Meding JB, Harty LD. The AGC all-polyethylene tibial component: a ten-year clinical evaluation. *J Bone Joint Surg Am.* 2003;85:489-93.
12. Hyldahl H, Regner L, Carlsson L, Kärholm J, Weidenhielm L. All-polyethylene vs. metal-backed tibial component in total knee arthroplasty—a randomized RSA study comparing early fixation of horizontally and completely cemented tibial components: part 1. Horizontally cemented components: AP better fixated than MB. *Acta Orthop.* 2005;76:769-77.
13. Ritter MA. The cemented all-poly tibia. *Orthopedics.* 1994;17:841.
14. Udomkiat P, Dorr LD, Long W. Matched-pair analysis of all-polyethylene versus metal-backed tibial components. *J Arthroplasty.* 2001;16:689-96.
15. Hamilton LR. UCI total knee replacement. A follow-up study. *J Bone Joint Surg Am.* 1982;64:740-4.
16. Rasquinha VJ, Ranawat CS, Cervieri CL, Rodriguez JA. The press-fit condylar modular total knee system with a posterior cruciate-substituting design. A concise follow-up of a previous report. *J Bone Joint Surg Am.* 2006;88:1006-10.
17. Rand JA, Ilstrup DM. Survivorship analysis of total knee arthroplasty. Cumulative rates of survival of 9200 total knee arthroplasties. *J Bone Joint Surg Am.* 1991;73:397-409.
18. Dixon MC, Brown RR, Parsch D, Scott RD. Modular fixed-bearing total knee arthroplasty with retention of the posterior cruciate ligament. A study of patients followed for a minimum of fifteen years. *J Bone Joint Surg Am.* 2005;87:598-603.
19. Engh GA, Dwyer KA, Hanes CK. Polyethylene wear of metal-backed tibial components in total and unicompartmental knee prostheses. *J Bone Joint Surg Br.* 1992;74:9-17.
20. Tsao A, Mintz L, McRae CR, Stulberg SD, Wright T. Failure of the porous-coated anatomic prosthesis in total knee arthroplasty due to severe polyethylene wear. *J Bone Joint Surg Am.* 1993;75:19-26.
21. Wright TM, Rimmnac CM, Stulberg SD, Mintz L, Tsao AK, Klein RW, McCrae C. Wear of polyethylene in total joint replacements. Observations from retrieved PCA knee implants. *Clin Orthop Relat Res.* 1992;276:126-34.
22. Conditt MA, Thompson MT, Usrey MM, Ismaili SK, Noble PC. Backside wear of polyethylene tibial inserts: mechanism and magnitude of material loss. *J Bone Joint Surg Am.* 2005;87:326-31.

23. Conditt MA, Stein JA, Noble PC. Factors affecting the severity of backside wear of modular tibial inserts. *J Bone Joint Surg Am.* 2004;86:305-11.
24. Engh GA, Lounici S, Rao AR, Collier MB. In vivo deterioration of tibial baseplate locking mechanisms in contemporary modular total knee components. *J Bone Joint Surg Am.* 2001;83:1660-5.
25. Parks NL, Engh GA, Topoleski LD, Emperado J. Modular tibial insert micromotion. A concern with contemporary knee implants. *Clin Orthop Relat Res.* 1998;356:10-5.
26. Rodriguez JA, Baez N, Rasquinha V, Ranawat CS. Metal-backed and allpolyethylene tibial components in total knee replacement. *Clin Orthop Relat Res.* 2001;392:174-83.
27. Wasielewski RC, Parks N, Williams I, Surprenant H, Collier JP, Engh G. Tibial insert undersurface as a contributing source of polyethylene wear debris. *Clin Orthop Relat Res.* 1997;345:53-9.
28. Gioe TJ, Sinner P, Mehle S, Ma W, Killeen KK. Excellent survival of allpolyethylene tibial components in a community joint registry. *Clin Orthop Relat Res.* 2007;464:88-92.
29. Muller SD, Deehan DJ, Holland JP, Outterside SE, Kirk LM, Gregg PJ, McCaskie AW. Should we reconsider all-polyethylene tibial implants in total knee replacement? *J Bone Joint Surg Br.* 2006;88:1596-602.
30. Bargren JH, Blaha JD, Freeman MA. Alignment in total knee arthroplasty. Correlated biomechanical and clinical observations. *Clin Orthop Relat Res.* 1983;173:178-83.
31. Bartel DL, Burstein AH, Santavicca EA, Insall JN. Performance of the tibial component in total knee replacement. *J Bone Joint Surg Am.* 1982;64:1026-33.
32. Bartel DL, Rawlinson JJ, Burstein AH, Ranawat CS, Flynn WF Jr. Stresses in polyethylene components of contemporary total knee replacements. *Clin Orthop Relat Res.* 1995;317:76-82.
33. Lewis JL, Askew MJ, Jaycox DP. A comparative evaluation of tibial component designs of total knee prostheses. *J Bone Joint Surg Am.* 1982;64:129-35.
34. Lotke PA, Ecker ML. Influence of positioning of prosthesis in total knee replacement. *J Bone Joint Surg Am.* 1977;59:77-9.
35. Reilly D, Walker PS, Ben-Dov M, Ewald FC. Effects of tibial components on load transfer in the upper tibia. *Clin Orthop Relat Res.* 1982;165:273-82.
36. Taylor M, Tanner KE, Freeman MA. Finite element analysis of the implanted proximal tibia: a relationship between the initial cancellous bone stresses and implant migration. *J Biomech.* 1998;31:303-10.
37. Walker PS, Greene D, Reilly D, Thatcher J, Ben-Dov M, Ewald FC. Fixation of tibial components of knee prostheses. *J Bone Joint Surg Am.* 1981;63:258-67.
38. Huiskes R. Some fundamental aspects of human joint replacement. Analyses of stresses and heat conduction in bone-prosthesis structures. *Acta Orthop Scand Suppl.* 1980;185:1-208.
39. National Joint Registry for England and Wales. 2nd annual report. September 2005. http://www.njrcentre.org.uk/NjrCentre/Portals/0/Documents/England/Reports/NJR_AR_2.pdf. Accessed 2009 Jun 2.
40. Gioe TJ, Killeen KK, Mehle S, Grimm K. Implementation and application of a community total joint registry: a twelve-year history. *J Bone Joint Surg Am.* 2006;88:1399-404.
41. Mendenhall S. Hospital resources and implant cost management—a 2008 update. *Orthop Network News.* 2009;20:13-9.
42. Babis GC, Trousdale RT, Morrey BF. The effectiveness of isolated tibial insert exchange in revision total knee arthroplasty. *J Bone Joint Surg Am.* 2002;84:64-8.
43. Engh GA, Koralewicz LM, Pereles TR. Clinical results of modular polyethylene insert exchange with retention of total knee arthroplasty components. *J Bone Joint Surg Am.* 2000;82:516-23.
44. Siddique MS, Rao MC, Deehan DJ, Pinder IM. Role of abrasion of the femoral component in revision knee arthroplasty. *J Bone Joint Surg Br.* 2003;85:393-8.
45. Bert JM, Reuben J, Kelly F, Gross M, Elting J. The incidence of modular tibial

- polyethylene insert exchange in total knee arthroplasty when polyethylene failure occurs. *J Arthroplasty*. 1998;13:609-14.
46. Callaghan JJ, Reynolds E, Lovell ME, Liu SS, Taylor SG, Goetz DD, Clohisy JC. Liner exchange and bone grafting for osteolysis and wear following total knee arthroplasty. Read at the Annual Meeting of the American Academy of Orthopaedic Surgeons; 2009 Feb 25-27; Las Vegas, NV.
47. Griffin WL, Scott RD, Dalury DF, Mahoney OM, Chiavetta JB, Odum SM. Modular insert exchange in knee arthroplasty for treatment of wear and osteolysis. *Clin Orthop Relat Res*. 2007;464:132-7.
48. Gioe TJ, Bowman KR. A randomized comparison of all-polyethylene and metalbacked tibial components. *Clin Orthop Relat Res*. 2000;380:108-15.
49. Gioe TJ, Stroemer ES, Santos ER. All-polyethylene and metal-backed tibias have similar outcomes at 10 years: a randomized level I [corrected] evidence study. *Clin Orthop Relat Res*. 2007;455:212-8. Erratum in: *Clin Orthop Relat Res*. 2007;458:249.
50. Burstein AH, Wright TM. Fundamentals of orthopaedic biomechanics. Baltimore: Williams and Wilkins; 1994. p 203-10.
51. Rao AR, Engh GA, Collier MB, Lounici S. Tibial interface wear in retrieved total knee components and correlations with modular insert motion. *J Bone Joint Surg Am*. 2002;84:1849-55.
52. Jayabalan P, Furman BD, Cottrell JM, Wright TM. Backside wear in modern total knee designs. *HSS J*. 2007;3:30-4.
53. Li S, Scuderi G, Furman BD, Bhattacharyya S, Schmieg JJ, Insall JN. Assessment of backside wear from the analysis of 55 retrieved tibial inserts. *Clin Orthop Relat Res*. 2002;404:75-82.
54. Cuckler JM, Lemons J, Tamarapalli JR, Beck P. Polyethylene damage on the nonarticular surface of modular total knee prostheses. *Clin Orthop Relat Res*. 2003;410:248-53.
55. Ritter MA, Meneghini RM. Twenty-year survivorship of cementless anatomic graduated component total knee arthroplasty. *J Arthroplasty*. 2009 May 6 [Epub ahead of print].
56. Weber AB, Worland RL, Keenan J, Van Bowen J. A study of polyethylene and modularity issues in >1000 posterior cruciate-retaining knees at 5 to 11 years. *J Arthroplasty*. 2002;17:987-91.
57. Himanen AK, Belt EA, Lehto MU, Hämäläinen MM. A comparison of survival of moulded monoblock and modular tibial components of 751 AGC total knee replacements in the treatment of rheumatoid arthritis. *J Bone Joint Surg Br*. 2007;89:609-14.
58. Brassard MF, Insall JN, Scuderi GR, Colizza W. Does modularity affect clinical success? A comparison with a minimum 10-year followup. *Clin Orthop Relat Res*. 2001;388:26-32.
59. Schwab JH, Haidukewych GJ, Hanssen AD, Jacofsky DJ, Pagnano MW. Flexion instability without dislocation after posterior stabilized total knees. *Clin Orthop Relat Res*. 2005;440:96-100.
60. Shannon BD, Klassen JF, Rand JA, Berry DJ, Trousdale RT. Revision total knee arthroplasty with cemented components and uncemented intramedullary stems. *J Arthroplasty*. 2003;18(7 Suppl 1):27-32.
61. Parratte S, Pagnano MW. Instability after total knee arthroplasty. *Instr Course Lect*. 2008;57:295-304.
62. Segawa H, Tsukayama DT, Kyle RF, Becker DA, Gustilo RB. Infection after total knee arthroplasty. A retrospective study of the treatment of eighty-one infections. *J Bone Joint Surg Am*. 1999;81:1434-45.
63. Marculescu CE, Berbari EF, Hanssen AD, Steckelberg JM, Harmsen SW, Mandrekar JN, Osmon DR. Outcome of prosthetic joint infections treated with debridement and retention of components. *Clin Infect Dis*. 2006;42:471-8.
64. Deirmengian C, Greenbaum J, Lotke PA, Booth RE Jr, Lonner JH. Limited success with open debridement and retention of components in the treatment of acute *Staphylococcus aureus* infections after total knee arthroplasty. *J Arthroplasty*. 2003;18(7 Suppl 1):22-6.
65. Silva M, Tharani R, Schmalzried TP. Results of direct exchange or debridement

- of the infected total knee arthroplasty. *Clin Orthop Relat Res.* 2002;404:125-31.
66. Bartel DL, Bicknell VL, Wright TM. The effect of conformity, thickness, and material on stresses in ultra-high molecular weight components for total joint replacement. *J Bone Joint Surg Am.* 1986;68:1041-51.
67. Wright TM, Fukubayashi T, Burstein AH. The effect of carbon fiber reinforcement on contact area, contact pressure, and time-dependent deformation in polyethylene tibial components. *J Biomed Mater Res.* 1981;15:719-30.
68. Edwards SA, Pandit HG, Ramos JL, Grover ML. Analysis of polyethylene thickness of tibial components in total knee replacement. *J Bone Joint Surg Am.* 2002;84:369-71.
69. Schai PA, Thornhill TS, Scott RD. Total knee arthroplasty with the PFC system. Results at a minimum of ten years and survivorship analysis. *J Bone Joint Surg Br.* 1998;80:850-8.
70. Murase K, Crowninshield RD, Pedersen DR, Chang TS. An analysis of tibial component design in total knee arthroplasty. *J Biomech.* 1983;16:13-22.
71. Nilsson KG, K arrholm J. RSA in the assessment of aseptic loosening. *J Bone Joint Surg Br.* 1996;78:1-3.
72. Ryd L, Albrektsson BE, Carlsson L, Dansg ard F, Herberts P, Lindstrand A, Regn er L, Toksvig-Larsen S. Roentgen stereophotogrammetric analysis as a predictor of mechanical loosening of knee prostheses. *J Bone Joint Surg Br.* 1995;77:377-83.
73. Adalberth G, Nilsson KG, Bystr om S, Kolstad K, Mallmin H, Milbrink J. Stability assessment of a moderately conforming all-polyethylene tibial component in total knee arthroplasty: a prospective RSA study with 2 years of follow-up of the Kinemax Plus design. *Am J Knee Surg.* 1999;12:233-40.
74. Adalberth G, Nilsson KG, Bystr om S, Kolstad K, Milbrink J. All-polyethylene versus metal-backed and stemmed tibial components in cemented total knee arthroplasty. A prospective, randomised RSA study. *J Bone Joint Surg Br.* 2001;83:825-31.
75. Adalberth G, Nilsson KG, Bystr om S, Kolstad K, Milbrink J. Low-conforming allpolyethylene tibial component not inferior to metal-backed component in cemented total knee arthroplasty: prospective, randomized radiostereometric analysis study of the AGC total knee prosthesis. *J Arthroplasty.* 2000;15:783-92.
76. Norgren B, Dal en T, Nilsson KG. All-poly tibial component better than metalbacked: a randomized RSA study. *Knee.* 2004;11:189-96.
77. Hyldahl H, Regn er L, Carlsson L, K arrholm J, Weidenhielm L. All-polyethylene vs. metal-backed tibial component in total knee arthroplasty—a randomized RSA study comparing early fixation of horizontally and completely cemented tibial components: part 2. Completely cemented components: MB not superior to AP components. *Acta Orthop.* 2005;76:778-84.
78. Hyldahl HC, Regn er L, Carlsson L, K arrholm J, Weidenhielm L. Does metal backing improve fixation of tibial component in unicondylar knee arthroplasty? A randomized radiostereometric analysis. *J Arthroplasty.* 2001;16:174-9.
79. Basset RW. Results of 1,000 Performance knees: cementless versus cemented fixation. *J Arthroplasty.* 1998;13:409-13.
80. Duffy GP, Berry DJ, Rand JA. Cement versus cementless fixation in total knee arthroplasty. *Clin Orthop Relat Res.* 1998;356:66-72.
81. Baker PN, Khaw FM, Kirk LM, Esler CN, Gregg PJ. A randomized controlled trial of cemented versus cementless press-fit condylar total knee replacement: 15-year survival analysis. *J Bone Joint Surg Br.* 2007;89:1608-14.
82. Swedish Knee Arthroplasty Register. <http://www.knee.nko.se/english/online/thePages/publication.php>. Accessed 2009 Jun 2.
83. Rand JA, Trousdale RT, Ilstrup DM, Harmsen WS. Factors affecting the durability of primary total knee prostheses. *J Bone Joint Surg Am.* 2003;85:259-65.
84. Gioe TJ, Killeen KK, Grimm K, Mehle S, Scheltema K. Why are total knee replacements revised? Analysis of early revision in a community knee implant registry. *Clin Orthop Relat Res.* 2004;428:100-6.
85. Gioe TJ, Novak C, Sinner P, Ma W, Mehle S. Knee arthroplasty in the young patient: survival in a community registry. *Clin Orthop Relat Res.* 2007;464:83-7.
86. Sharkey PF, Sethuraman V, Hozack WJ, Rothman RH, Stiehl JB. Factors influencing

- choice of implants in total hip arthroplasty and total knee arthroplasty: perspectives of surgeons and patients. *J Arthroplasty*. 1999;14:281-7.
87. Clark CR. Cost containment: total joint implants. *J Bone Joint Surg Am*. 1994;76:799-800.
88. American Academy of Orthopaedic Surgeons. Position statement. Value driven use of orthopaedic implants. <http://www.aaos.org/about/papers/position/1104.asp>. Accessed 2009 Jun 2.
89. Containing the cost of orthopaedic implants. *Am Acad Orthop Surg Bull*. 1996;44:23.
90. Healy WL, Iorio R, Ko J, Appleby D, Lemos DW. Impact of cost reduction programs on short-term patient outcome and hospital cost of total knee arthroplasty. *J Bone Joint Surg Am*. 2002;84:348-53.
91. Najibi S, Iorio R, Surdam JW, Whang W, Appleby D, Healy WL. All-polyethylene and metal-backed tibial components in total knee arthroplasty: a matched pair analysis of functional outcome. *J Arthroplasty*. 2003;18(7 Suppl 1):9-15.
92. Pomeroy DL, Schaper LA, Badenhausen WE, Suthers KE, Smith MW, Empson JA, Curry JI. Results of all-polyethylene tibial components as a cost-saving technique. *Clin Orthop Relat Res*. 2000;380:140-3.
93. Pagnano MW, Levy BA, Berry DJ. Cemented all polyethylene tibial components in patients age 75 years and older. *Clin Orthop Relat Res*. 1999;367:73-80.
94. Wilson NA, Schneller ES, Montgomery K, Bozic KJ. Hip and knee implants: current trends and policy considerations. *Health Aff (Millwood)*. 2008;27:1587-98.
95. Rastogi A, Mohr BA, Williams JO, Soobader MJ, de Brantes F. Prometheus payment model: application to hip and knee replacement surgery. *Clin Orthop Relat Res*. 2009;467:2587-97.
96. Insall JN, Dorr LD, Scott RD, Scott WN. Rationale of the Knee Society clinical rating system. *Clin Orthop Relat Res*. 1989;248:13-4.
97. Dawson J, Fitzpatrick R, Murray D, Carr A. Questionnaire on the perceptions of patients about total knee replacement. *J Bone Joint Surg Br*. 1998;80:63-9.
98. Ware J Jr, Kosinski M, Keller SD. A 12-Item Short-Form Health Survey: construction of scales and preliminary tests of reliability and validity. *Med Care*. 1996;34:220-33.
99. Goe TJ, Glynn J, Sembrano J, Suthers K, Santos ER, Singh J. Mobile and fixedbearing (all-polyethylene tibial component) total knee arthroplasty designs. A prospective randomized trial. *J Bone Joint Surg Am*. 2009;91:2104-12.
100. WOMAC Osteoarthritis Index. Knee and Hip Osteoarthritis Index. <http://www.womac.org/womac/index.htm>. Accessed 2009 Jun 2.
101. Ware JE Jr, Sherbourne CD. The MOS 36-item short-form health survey (SF-36). I. Conceptual framework and item selection. *Med Care*. 1992;30:473-83.
102. L'Insalata JL, Stern SH, Insall JN. Total knee arthroplasty in elderly patients. Comparison of tibial component designs. *J Arthroplasty*. 1992;7:261-6.
103. Rand JA. Comparison of metal-backed and all-polyethylene tibial components in cruciate condylar total knee arthroplasty. *J Arthroplasty*. 1993;8:307-13.
104. Ma HM, Lu YC, Ho FY, Huang CH. Long-term results of total condylar knee arthroplasty. *J Arthroplasty*. 2005;20:580-4.
105. Shen B, Yang J, Zhou Z, Kang P, Wang L, Pei F. Survivorship comparison of allpolyethylene and metal-backed tibial components in cruciate-substituting total knee arthroplasty—Chinese experience. *Int Orthop*. 2008;33:1243-7.
106. Ranawat AS, Mohanty SS, Goldsmith SE, Rasquinha VJ, Rodriguez JA, Ranawat CS. Experience with an all-polyethylene total knee arthroplasty in younger, active patients with follow-up from 2 to 11 years. *J Arthroplasty*. 2005;20(7 Suppl 3):7-11.
107. Galvin AL, Kang L, Udofia I, Jennings LM, McEwen HM, Jin Z, Fisher J. Effect of conformity and contact stress on wear in fixed-bearing total knee prostheses. *J Biomech*. 2009;42:1898-902.
108. Stiehl JB, Komistek RD, Dennis DA. Detrimental kinematics of a flat on flat total condylar knee arthroplasty. *Clin Orthop Relat Res*. 1999;365:139-48.